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FT-IR Characterization of Antimicrobial Hybrid Materials through Sol-Gel Synthesis

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Received: 5 January 2020; Accepted: 6 February 2020; Published: 10 February 2020

Abstract: Silica/polycaprolactone and titania/polycaprolactone hybrid organic/inorganic amorphous composites were prepared via a sol-gel method starting from a multi-element solution containing tetramethyl orthosilicate (TMOS) or titanium butoxide (TBT), polycaprolactone (PCL), water and methylethylketone (MEK). The molecular structure of the crosslinked network was based on the presence of the hydrogen bonds between organic/inorganic elements as confirmed by Fourier Transform Infra-Red (FT-IR) analysis. In particular, the structure of crosslinked network was realized by hydrogen bonds between the X-OH (X = Si or Ti) group (H donator) in the sol-gel intermediate species and ester groups (H-acceptors) in the repeating units of the polymer. The morphology of the hybrid materials; pore size distribution, elemental homogeneity and surface features, was studied by scanning electron microscopy/energy dispersive spectroscopy (SEM/EDS) and by atomic force microscopy (AFM). The bioactivity of the synthesized hybrid materials was confirmed by observing the formation of a layer of hydroxyapatite (HAP) on the surface of the samples soaked in a simulated body fluid. The antimicrobial behavior of synthesized hybrids was also assessed against *Escherichia coli* bacteria. In conclusion, the prepared hybrid materials are proposed for use as future bone implants.

Keywords: hybrid composite; PCL; TiO₂; SiO₂; FT-IR spectroscopy; antibacterial behavior

1. Introduction

Since the 1990s, organic/inorganic nanocomposites networks have become a growing field of investigation [1–3]. The sol-gel route represents an interesting approach, which can be effectively applied to the preparation of the inorganic phases within the inorganic/organic hybrid materials, due to the fact that it can occur in liquid solutions at room temperature. These materials are considered to be biphasic, where the organic and inorganic phases are mixed at the nanometric or submicronic scales. The smaller the scale of mixing, the more unexpected the properties are, since these materials may show properties that are not the sum of the individual contributions from both phases. Additionally, it has been proved that the role of the inner interfaces is predominant; in particular, the nature of the interface is the critical parameter used to distinguish two different classes [4]: class I collects those hybrid materials with weak bonds (hydrogen, van der Waals or ionic bonds), and class II gathers materials where the phases are linked together through strong chemical bonds (covalent or ionic-covalent bonds). In class I, materials, obtained combining the sol-gel process with polymer chemistry, can be enclosed with a large number of different applications [5–7], from non-linear optical materials [8] to mesoporous materials [9].

The basic chemical reactions of the sol-gel process are the hydrolyses of metal alkoxides in the proper solvent, usually an alcohol/water mixture, followed by their polycondensation. In the first stage, substituting the alkoxide groups (OR) with the hydroxyl groups (OH) in the metal alkoxide offers a large number of opportunities, due to the presence of such reactive OH groups, to match with organic monomers. Thus, a variety of organic polymers have been introduced into inorganic networks. The final material derives from the condensation of two OH groups with the elimination of a water molecule. The two adjacent OH groups may belong to one organic and one inorganic monomer to afford the formation of a hybrid or composite material with covalent bonds between the polymer and inorganic elements. The gel reaction might also give rise to weaker bonds, such as a hydrogen bond, in the organic/inorganic hybrid bulky materials. It is well known that many parameters, such as type and concentration of reactants, solvents, catalysts, reaction temperature and removal rate of by-products and solvents, influence the sol-gel process [10,11]. Hence, it is evident that the presence of organic elements modifies the morphology and physical properties of the final sol-gel products. The difference in products that are obtained through the base-catalyzed sol-gel reaction and through the carefully controlled acid-catalyzed one is evident, since from the first process, translucent or opaque products with visible organic/inorganic phase separation are obtained, while from the second, transparent and monolithic materials are realized. A key topic that is persistently challenging in these organic-altered materials is the degree of mixing of the organic/inorganic elements, i.e., the phase homogeneity. The high optical transparency to visible light suggests that the organic/inorganic phase separation, if any, occurs on a scale of ≤ 400 nm [12]. Two of the most-used techniques to investigate phase mixing in hybrid materials, at micrometric scale, are atomic force microscopy (AFM) [13] and scanning electron microscopy (SEM).

In this work, we propose a combination of bioactive organic and inorganic phases to obtain a single and homogeneous hybrid composite using the sol-gel route for the inorganic three-dimensional (3D) network. In particular, we chose SiO_2 and TiO_2 -containing bioactive materials that are often produced in the amorphous state, typical of glasses, via the sol-gel route. Both of these oxides are known to bond to living bone [14]. Thus, a hybrid material based on smart combinations of biodegradable polymers, specifically polycaprolactone (PCL), and such bioactive inorganic compounds is of particular interest, since it exhibits tailored physical, biological and mechanical properties, as well as predictable degradation behavior.

The purpose of this manuscript is the microstructural characterization and bioactivity assessment of polycaprolactone/ SiO_2 and polycaprolactone/ TiO_2 hybrid materials prepared by the sol-gel process. These materials were tested in simulated body fluid (SBF) to prove their bioactivity in vitro [15] since the organic element, PCL, was preferred due to its biodegradable and biocompatible nature. Furthermore, as implant failure is often a consequence of microbial infections that occur in spite of antimicrobial prophylaxis and aseptic working conditions, the antimicrobial capability of the synthesized hybrids was investigated through a diffusion method against Gram-positive *Escherichia coli* after 24 h of incubation.

2. Materials and Methods

Organic/inorganic hybrid materials MO_2/PCL with $\text{M} = \text{Si}$ or Ti were prepared, using the sol-gel process, from polycaprolactone of analytical reagent grade as the organic element, and tetramethyl orthosilicate (TMOS) as the source for SiO_2 , or titanium butoxide as the source for TiO_2 . The amount of the organic element was 6 wt.% in both PCL/ SiO_2 and PCL/ TiO_2 hybrid materials, as optimized in a previous work [15].

In Figure 1, the flow chart of hybrid synthesis by the applied sol-gel route is depicted.

The presence of hydrogen bonds between organic/inorganic elements of the hybrid materials was unraveled by acquiring their FT-IR spectra in the $400\text{--}4000\text{ cm}^{-1}$ region using a Prestige 21 (Shimadzu, Kyoto, Japan) system with a resolution of 4 cm^{-1} (45 scans). The spectrometer used a Deuterated Triglycine Sulfate (DTGS) detector with KBr windows. Disks with a diameter of 13 mm, a thickness of 2 mm, a weight of 200 mg and containing 1 wt.% of sample in KBr were obtained by pressing sample

powders into a cylindrical holder using a Specac manual hydraulic press. The Prestige software (IR solution) was used to analyze the FT-IR spectra.

Figure 1. Flow chart of PCL/SiO₂ and PCL/TiO₂ gel synthesis.

The nature of MO₂ gel, PCL and PCL/MO₂ hybrid materials was confirmed by X-ray diffraction (XRD) analysis using a Philips diffractometer. Powder samples were scanned from $2\theta = 5^\circ$ to 60° using CuK α radiation.

The surface morphology and phase distribution of the organic/inorganic hybrid materials were investigated by a scanning electron microscope (Cambridge model S-240) and by an atomic force microscope (Digital Instruments Multimode) in contact mode in air. For SEM, the specimens were previously coated with a thin Au film to obtain a conductive surface.

Bioactivity tests were performed on pieces of the hybrid materials soaked in a simulated body fluid (SBF) with the proper ion concentrations [16,17] nearly equal to those of human blood plasma. During soaking, the temperature was fixed at 37 °C and the ratio between the exposed surface and the volume solution was kept constant (50 mm² mL^{−1} of solution), due to its strong influence on the reactivity degree, as previously reported [17–19].

The ability of the hybrid materials to form an apatite layer during the SBF soaking test was ascertained by FT-IR analysis on SiO₂/PCL-reacted samples, where SEM and EDS analyses were performed on TiO₂/PCL-reacted samples. An SEM outfitted with an energy-dispersive X-ray fluorescence system (EDS, Link AN10000, Oxford Microanalysis) was used to investigate the morphology of the coated sample and to complete it with qualitative elemental analysis.

The antimicrobial activity of synthesized materials was investigated by a diffusion method. *Escherichia coli* (ATCC 25,922) bacteria culture was diluted in distilled water to achieve a 1.0×10^6 CFU/mL suspension. This latter was inoculated in Tryptone Bile Glucuronide Agar (TBX) medium (Liofilchem, Roseto degli Abruzzi (TE), Italy). Sample hybrids and a control disk were placed at the center of the Petri dishes using a pair of sterile tweezers. Incubation was carried out for 24 h in an incubator at 44 °C. The microbial growth was evaluated by observing the diameter of the inhibition halo (ID). Antimicrobial tests were performed in quadruplicate on different days to ensure reproducibility, and values are expressed as the mean values $\pm$ standard deviation (SD) of all the performed measurements.

3. Results and Discussion

Gelation is the result of hydrolysis and condensation according to the following reactions, where $M = \text{Si}$ and $R = \text{CH}_3$ for PCL/SiO₂; and $M = \text{Ti}$ and $R = \text{C}_4\text{H}_9$ for PCL/TiO₂.

The reaction mechanism is not known in great detail; however, it is generally accepted that it proceeds through a second-order nucleophilic substitution [19]. The reaction (4) shows the formation of the organic/inorganic network in which a hydrogen bond between the ester C=O group of the organic polymer and the inorganic matrix was supposed to occur. Indeed, the carbonyl group of the polymer chain acts as an H-acceptor, whereas the O-H group of the inorganic matrix is the H-donor.

In Figure 2, FT-IR spectra of pure PCL and SiO₂ are reported, together with the one recorded for SiO₂/PCL_{6 wt.%} gel in order to highlight spectral differences due to the interaction of the two phases. The PCL spectrum (Figure 2a) shows the asymmetric and symmetric stretching of polymer -CH₂-groups, corresponding to the bands at 2945 and 2866 cm⁻¹, respectively, and two peaks at 1470 cm⁻¹ and 1360 cm⁻¹ related to their bending modes. The sharp and strong band at 1730 cm⁻¹ referred to the C=O stretching vibration. On the other hand, the hybrid's FT-IR spectrum (Figure 2b) showed a broad band in the range 3600–3200 cm⁻¹, the intensity of which almost completely covered the characteristic peaks of PCL methylene stretching. According to previous work, this referred to un-free O-H groups and could be explained considering the establishment of hydrogen bonds between the carbonyl groups of the polymer chains and the inorganic part [11]. The shift of the pure PCL signal at 1730 cm⁻¹ to lower wavenumbers (1720 cm⁻¹) seemed to corroborate this hypothesis. Moreover, both in SiO₂/PCL_{6 wt.%} and SiO₂ gel spectra (Figure 2b,c), the bands at 1080 and 460 cm⁻¹, corresponding to the stretching and bending modes of SiO₂ tetrahedra [20], were marked, as expected. This evidence indicates that the presence of the PLC in the hybrid composites does not inhibit the reticulation of the Si-O-Si 3D network.

In Figure 3, the infrared spectrum of PCL, as discussed above, was compared to those recorded for the TiO₂ + PCL_{6 wt.%} gel and the TiO₂ gel. The signals detectable for the latter were the typical bands already described elsewhere [3]. In the hybrid's spectrum (Figure 3b), the broad and strong band in the region 3400–3200 cm⁻¹, due to -OH vibrations, obscured almost completely the polycaprolactone CH₂ asymmetric and symmetric stretching modes (at 2945 and 2866 cm⁻¹, respectively). In addition, the band at 1715 cm⁻¹, attributable to the PCL ester bond, which shifted to low wavenumbers following the synthetic route, was not particularly evident. The scarce intensity could depend on the low amount of the polymer in the synthesized material. Furthermore, other signals typical of acetic-acid-containing titania sol-gel materials were detected. Indeed, the doublet at 1530 and 1445 cm⁻¹ likely corresponded to the asymmetric and symmetric stretching vibrations of the carboxylic group coordinated to Ti as a bidentate ligand. The band around 800 cm⁻¹ correlates with the vibrations of polyhedral TiOn with a coordination number less than 6.

Figure 2. FT-IR spectra of (a) PCL, (b) $\text{SiO}_2 + \text{PCL}_6 \text{ wt.}\%$ gel and (c) SiO_2 gel.

Figure 3. FT-IR spectra of (a) PCL, (b) $\text{TiO}_2 + \text{PCL}_6 \text{ wt.}\%$ gel and (c) TiO_2 gel.

The nature and microstructure of the SiO_2/PCL and TiO_2/PCL hybrid materials were investigated by X-ray diffraction (XRD) and scanning electron microscopy (SEM). In particular, based on the acquired diffractograms, hybrids exhibit amorphous features as their metal oxide precursors. In fact, taking into account Figure 4, it is observable that sharp peaks, typical of a crystalline material, can be detected on the diffractogram of pure polycaprolactone (Figure 4a), whereas the TiO_2 gel exhibits broad humps characteristic of amorphous materials (Figure 4b). On the other hand, the XRD spectrum of the TiO_2/PCL hybrid material gel was in line with an amorphous material, such as TiO_2 gel (Figure 4c).

Figure 4. XRD spectra of (a) PCL, (b) TiO_2 gel and (c) TiO_2/PCL gel.

SEM micrographs of TiO_2 gel and TiO_2/PCL gel samples, reported in Figure 5, evidence a more homogenous morphology for the first one, as expected. With the introduction of the organic phase (Figure 5b), the unstructured TiO_2 gel presents a micrometric feature. Neither of the two morphologies, though, exhibit a regular geometric morphology indicating crystalline structures or phase separation. This result confirms the XRD evidence, i.e., the crystalline nature of the organic element was lost during the synthesis. A similar behavior was detected on XRD patterns and SEM micrographs of a SiO_2 gel sample and a SiO_2/PCL gel sample.

Figure 5. Scanning electron microscopy (SEM) micrograph of (a) TiO_2 gel and (b) $\text{TiO}_2/\text{PCL}_{6 \text{ wt.}\%}$ gel.

The degree of mixing of the elements in the hybrid material was investigated with Atomic Force microscopy (AFM). An AFM contact mode image can be measured in the height mode or in the force mode. In force images (z range in nN), differences appear sharper and richer and the contours of the nanostructure's essentials are clearer. In contrast, height images (z range in nm) provide a more exact reproduction of the height itself [21]. In this study, the height mode was adopted to estimate the degree of homogeneity of the hybrid materials. AFM topographic images of SiO_2/PCL and TiO_2/PCL gel samples are shown in Figure 6, where it can be observed that the average domain size is less than 130 and 40 nm. This answer confirms that the synthesized SiO_2/PCL and TiO_2/PCL gels can intrinsically be organic/inorganic hybrid materials [22].

Figure 6. AFM images showing the microstructure of (a) $\text{SiO}_2/\text{PCL}_{6 \text{ wt.}\%}$ gel and (b) $\text{TiO}_2/\text{PCL}_{6 \text{ wt.}\%}$ gel. The numbers on the axis are in μm (micrometers).

The bioactivity of the SiO_2/PCL gel was ascertained by FT-IR measurements on a sample soaked in simulated body fluid for 7, 14 and 21 days as shown in Figure 7. The formation of a hydroxyapatite deposit was recognized by the appearance of the 587 and 550 cm^{-1} bands generally assigned to P-O stretching [23]. After soaking for 7 days, the splitting of the 580 cm^{-1} band into two others at 587 and at 550 cm^{-1} can be ascribed to the shape of crystalline hydroxyapatite [23]. These spectra modifications could be ascribable to the formation of the hydroxyapatite precipitate and, in particular, to the stretching of the hydroxyapatite -OH groups and the vibrations of PO_4^{3-} groups, respectively [24]. Moreover, a slight upshift of the Si-OH band (from 955 cm^{-1} to 960 cm^{-1}) suggested the interaction of the hydroxyapatite layer with the -OH groups of the silica matrix. Finally, the band at 800 cm^{-1} can be assigned to the Si-O-Si band vibration among two adjacent tetrahedra characteristic of silica gel [24]. The results obtained are in line with the mechanism of the formation of a hydroxy apatite deposit proposed in the literature [25].

Figure 7. FT-IR spectra of SiO_2/PCL gel samples after exposure to simulated body fluid (SBF) for different times. (a) not exposed; (b) 7 days; (c) 14 days; (d) 21 days.

Figure 8a shows the SEM micrographs of a TiO_2/PCL gel sample soaked in SBF for 21 days. Figure 8b confirms that the surface layer observed in the SEM micrographs is composed of calcium phosphate.

Figure 8. (a) SEM micrographs and (b) EDS of a TiO₂/PCL gel sample soaked in SBF for 21 days.

Finally, in order to propose the use of the synthesized materials in the biomedical field, as microbial infections can compromise the effectiveness and success of implants, preliminary data from a diffusion assay highlighted that TiO₂/PCL_{6 wt.%} materials exerted a strong inhibitory effect against *Escherichia coli* growth (Figure 9). *E. coli*, a Gram-negative bacterium, being able to easily adapt to changing environmental conditions, is one of the primary causes of Gram-negative orthopedic implant infections. Its resistance to a great variety of antibiotics does not allow for its successful eradication even after treatment. Thus, antimicrobial materials could be advantageous in the biomedical field. Indeed, the significant antimicrobial effect of TiO₂/PCL_{6 wt.%} could be substantially due to the TiO₂ element. In fact, previous findings state that TiO₂ nanoparticles found on pathogenic strains of *E. coli* were able to cause little pores to form in bacterial cell walls, leading to increased permeability and cell death [26].

Figure 9. Representative image of *Escherichia coli* incubated with synthesized hybrid materials and antimicrobial activity reported as inhibitory zone diameter (mm).

4. Conclusions

MO₂/PCL materials, based on polycaprolactone and silica or titanium metal oxide (M = Si or Ti), prepared via the sol-gel process, were found to be organic/inorganic bioactive hybrid materials not altering the gelification and condensation route of the inorganic gel. The polymer (PCL) was crosslinked to the network by hydrogen bonds, as ascertained by FTIR spectra, between the ester groups of the organic polymer and the hydroxyl groups of inorganic matrices. Moreover, the AFM and SEM analyses confirmed that MO₂/PCL can be considered to be homogenous organic/inorganic hybrid materials because the average domains are less than 400 nm in size. Finally, the bioactivity of the PCL/MO₂ materials was ascertained by the formation of a layer of hydroxyapatite on the surface when samples were soaked in SBF, as shown in SEM micrographs and related EDS and detected in FTIR spectra. Although further investigations are required for evaluating the mechanical properties of the synthesized hybrid materials, these findings provide initial evidence of the strong antimicrobial effect of the TiO₂/PCL hybrid and its potential for favorable use.

Author Contributions: Conceptualization, M.C.; methodology, S.P. and M.C.; software, C.L.; validation, M.C., C.L. and formal analysis, S.P. and M.C.; investigation, M.C.; resources, C.L.; data curation, M.C.; writing—original draft preparation, M.C. and C.L.; writing—review and editing, M.C.; visualization, C.L.; supervision, M.C. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Acknowledgments: The authors thank the Ecoricerche srl company for making the microbiology laboratories and materials used for experiments available.

Conflicts of Interest: The authors declare no conflicts of interest.

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