Abstract: Renal hypoxia has recently been implicated as a key contributor and indicator of various glomerular diseases. As such, monitoring changes in renal oxygenation in these disorders may provide an early diagnostic advantage that could prevent potential adverse outcomes. Blood oxygen level-dependent magnetic resonance imaging (BOLD MRI) is an emerging noninvasive technique for assessing renal oxygenation in glomerular disease. Although BOLD MRI has produced promising initial results for the use in certain renal pathologies, the use of BOLD imaging in glomerular diseases, including primary and secondary nephrotic and nephritic syndromes, is relatively unexplored. Early BOLD studies on primary nephrotic syndrome, nephrotic syndrome secondary to diabetes mellitus, and nephritic syndrome secondary to systemic lupus erythematosus have shown promising results to support its future clinical utility. In this review, we outline the advancements made in understanding the use of BOLD MRI for the assessment, diagnosis, and screening of these pathologies.

Keywords: BOLD MRI; glomerular; hypoxia; nephrotic; nephritic

1. Introduction

Glomerular disease continues to be a large health burden worldwide, often occurring as a primary process or as secondary to systemic inflammatory conditions, infections, and diabetes mellitus [1]. In the past 10 years, multiple studies have implicated renal hypoxia in glomerular disease [2–4]. These studies indicate that patients with glomerular disease exhibit significant decreases in both renal blood flow and oxygenation, possibly due to basement membrane thickening and extracellular collagen deposition in the mesangium [5]. In order to reduce potential adverse outcomes, monitoring renal hypoxia may establish an early diagnosis and even help monitor disease progression. A novel noninvasive method currently being investigated for such purposes is blood oxygenation level-dependent magnetic resonance imaging (BOLD MRI), a functional MRI (fMRI) technique that can evaluate organ function on the basis of differences in the magnetic properties of deoxyhemoglobin and hemoglobin. BOLD MRI operates by detecting the differing paramagnetic spin states of deoxyhemoglobin versus oxyhemoglobin. Increasing amounts of deoxyhemoglobin induce an internal magnetic field and phase dispersions of neighboring spin states, which ultimately distorts the MRI signal. These results are reported as the R2* (sec$^{-1}$) value, which is the apparent relaxation rate and indicates the relative content of deoxymoglobin. Higher R2* values are inversely correlated with tissue oxygenation and vice versa. For example, tissue areas receiving increased blood flow have a decreased proportion of deoxyggenated hemoglobin, and thus, a lower apparent relaxation rate R2*. 
BOLD MRI has been a cornerstone in neuroimaging since the early 1990s, giving clinicians the ability to measure areas of the brain affected by ischemia [6]. Neurologists and neurosurgeons consistently employ BOLD as a primary fMRI technique, often using it for pre-operative analysis as well as other applications such as seizure tracking [7]. Such extensive use in neurology clinics, as well as in research, is responsible for most of our current understanding of the best data acquisition methods for BOLD MRI. However, this technological and scientific understanding is relatively specific to cerebrovascular imaging. With the clear physiological differences between the brain and kidney, specific techniques and settings for renal imaging are needed. This has led to the investigation of BOLD MRI’s utility in renal disease, especially chronic kidney disease (CKD) and renal artery stenosis. As both pathologies involve hypoxia, BOLD MRI may be an effective tool to track disease progression [8]. Furthermore, these studies have found that for renal BOLD imaging, a multiple gradient-recalled-echo (mGRE) sequence has a superior signal-to-noise ratio and resolution compared to a spin-echo sequence [9]. These BOLD MRI results are commonly analyzed using region of interest (ROI) analysis to assess medullary R2* (mR2*) and cortical R2* (cR2*) values, giving physicians important insights into the respective oxygenation of the kidney. Another method being investigated is the twelve-layer concentric objects (TLCO) technique, which may have better accuracy than ROI analysis in advanced disease (Figure 1) [10].

![Figure 1. Demonstration of blood oxygenation level-dependent magnetic resonance imaging (BOLD MRI) kidney visualization. (A) Region of interest (ROI) technique with circles demonstrating ROIs, and (B) Twelve-layer concentric objects (TLCO) technique. (Figure reprinted with permission from Oxford Academic, from Prujim et al., 2018).](image-url)

Interestingly, emerging literature now indicates that BOLD MRI can also be used for glomerular disease diagnosis and management. In contrast to anatomical methods such as sonography, BOLD MRI provides clinicians with a more effective ability to functionally evaluate early changes in nephrotic and nephritic syndromes, encompassing both primary and secondary etiologies. The capability to noninvasively assess renal oxygenation makes it a highly attractive option for use in the clinical setting. Given that renal tissue hypoxia plays a major role in the development of primary and secondary glomerular disease, BOLD MRI could play an important role by allowing for earlier identification and initiation of treatment. As imaging does not currently play a significant role in the diagnosis or management of such diseases, BOLD MRI has the potential to change current clinical guidelines. Here, we review recent advances made in BOLD MRI’s use in primary nephrotic syndrome, secondary nephrotic syndrome due to diabetes mellitus, and secondary nephritic syndrome due to systemic lupus erythematosus (SLE).
2. Primary Nephrotic Syndrome

Primary nephrotic syndrome (PNS) is a collection of symptoms that result from glomerular basement membrane damage, leading to shared features of proteinuria, hyperlipidemia, hypercoagulability, hypogammaglobulinemia, and hypoalbuminemia. Causes of PNS include minimal change disease (MCD), membranous glomerulonephritis (MGN), and focal segmental glomerulosclerosis (FSGS). Abnormal intrarenal oxygenation patterns and consequent hypoxia associated with primary nephrotic syndrome have spurred investigations into BOLD MRI’s use in these disorders.

As mentioned, medullary R2* values in BOLD MRI are used as a marker for medullary oxygen concentration, with several studies correlating lower mR2* values with primary nephrotic syndrome progression. Recent research showed that patients with various causes of primary nephrotic syndrome had significantly lower mR2* values compared to controls. Their mR2* values were also negatively correlated with estimated glomerular filtration rate (eGFR) and positively correlated with tubulointerstitial lesions [11]. The significantly lower mR2* seen in PNS patients may be secondary to reduced sodium reabsorption, and thus, reduced oxygen consumption, as well as enhanced oxyhemoglobin concentrations within inflammatory and immune-mediated kidney injuries [11–13]. Furthermore, correlations of mR2* with eGFR highlight the potential for BOLD MRI to be used clinically in PNS patients to evaluate their kidney function and prognosis [11,14].

Another recent study showed that higher cR2* values correlated positively with hypoxia and renal impairment in a sample of 29 patients with CKD, 9 of whom had underlying membranous glomerulonephritis [5]. Given that these findings were in CKD patients, of whom a large proportion had membranous glomerulonephritis, further investigation into an isolated patient population of those with MGN or other PNS is warranted. Such studies would help to support the use of BOLD MRI in the clinical setting for monitoring renal function in patients with PNS.

3. Nephrotic Syndrome Secondary to Diabetes Mellitus

Uncontrolled diabetes mellitus can lead to diabetic nephropathy (DN), which can later present as a secondary nephrotic syndrome. Development of nephrotic syndrome in diabetic patients involves multiple mechanisms and signaling pathways, including increased extracellular matrix deposition at the glomerular basement membrane. Long-standing diabetic nephropathy can lead to persistent albuminuria that depletes serum albumin, leading to edema and other classical symptoms of nephrotic syndrome [15]. The increased prevalence of secondary nephrotic syndrome due to diabetes has made screening for DN imperative. Testing for microalbuminuria has been a commonly used screening test in diabetic patients, but several studies have demonstrated that microalbuminuria often resolves in early stage DN patients and may not be an accurate biomarker [16–18]. While the introduction of contiguous tests, such as albumin to creatinine ratios, has attempted to increase the accuracy of screening and diagnosis, there is still room for innovation in this constantly developing area. Such potential makes BOLD MRI a highly attractive noninvasive alternative to evaluate DN progression.

To this end, several studies have attempted to correlate BOLD MRI results with DN progression in order to monitor the disease before its development to nephrotic syndrome (Figure 2). One BOLD MRI study found that mR2* values were highest in diabetic patients with normoalbuminuria when compared to healthy patients and diabetic patients with microalbuminuria, suggesting that medullary hypoxia may resolve with DN progression [19]. These results are in contrast to another study by Wang et al., which found that mR2* values in DN patients were significantly lower than those in healthy patients (Figure 2) [20]. This discrepancy may be explained by the fact that advanced DN reduces the glomerular filtration rate, in turn decreasing sodium transport and renal oxygen usage [20]. A higher kidney oxygenation (lower mR2* values) occurs as a result, which may reconcile with the lower mR2* values found in Feng et al.’s moderately microalbuminuric patients.
There is a greater degree of contrast between the cortex and medulla of the healthy patient compared to the diabetic patient, indicating decreased mR2* values that result in reduced contrast. (Figure reprinted with permission from Wiley, from Wang et al., 2011).

However, other studies that examine the impact of drugs on DN patients still use lower mR2* values as an indicator of success. One study found that DN patients who received lipo-prostaglandin E1 had significant decreases in mR2* values due to a reduction in tissue hypoxia following 14 days of treatment, compared to no significant differences in non-diabetic CKD patients [21]. Pruijm et al. administered angiotensin-converting enzyme inhibitors and angiotensin II receptor blockers to patients with diabetic kidney disease to explore the utility of BOLD MRI [22]. Unlike Li et al., they found that a renin–angiotensin–aldosterone system (RAAS) blockade did not induce significant change in R2* values [22]. The authors suggested that hypoxia is not involved in early diabetic nephropathy, which is in direct contrast to Feng et al.’s conclusions. Given the heterogeneity of results, more studies are needed in order to fully explore the clinical use of BOLD MRI in assessment of diabetic nephropathy progression.

4. Nephritic Syndrome Secondary to Systemic Lupus Erythematosus

Systemic lupus erythematosus (SLE) is a complex disease that can affect nearly every organ system in the body. One of the deadliest manifestations is lupus nephritis (LN), a secondary glomerular disease that affects more than 60,000 Americans and is seen in more than 30% of SLE patients [23,24]. SLE patients often undergo frequent urinalysis, including urine protein excretion and sedimentation, in order to detect early manifestations of nephritis. An abnormal urinalysis raises suspicion for LN and may guide a physician’s decision to pursue a biopsy. Diagnosis and personalized treatment are often guided by biopsy, which classifies renal involvement using the International Society of Nephrology and the Renal Pathology Society (ISN/RPS) guidelines (Figure 3). LN can present as several

Figure 2. Representative BOLD MRI images of healthy and diabetic nephropathy patients. (a,b) Gradient-recalled-echo maps and R2* maps of a healthy patient, respectively. (c,d) Gradient-recalled-echo maps and R2* maps of a patient with diabetic nephropathy, respectively. There is a greater degree of contrast between the cortex and medulla of the healthy patient compared to the diabetic patient, indicating decreased mR2* values that result in reduced contrast. (Figure reprinted with permission from Wiley, from Wang et al., 2011).
different subtypes of both nephrotic and nephritic syndromes, and most commonly presents as diffuse proliferative nephritis, a type of nephritic syndrome. For simplicity’s sake, we grouped LN under secondary nephritic syndrome, as its most common manifestation is diffuse proliferative glomerulonephritis, a nephritic syndrome. It is worth acknowledging that LN can present as a nephrotic syndrome, and some of the following studies use a patient sample that has a mixed population of LN subtypes.

Unfortunately, many patients undergo multiple biopsies in the years after diagnosis in order to track the disease progression and monitor the response to treatment, increasing both the cost and inconvenience to the patient. This has driven the investigation into BOLD MRI’s potential use for diagnosis and monitoring of lupus nephritis. Several early landmark studies have shown promising results. Li et al. demonstrated that cR2* and mR2* values were significantly lower in LN patients than in healthy controls [25]. In contrast, two recent studies by Rapacci et al. and Shi et al. did not find significant associations between cortical or medullary R2* values and the disease state [26,27]. This contrast may be due to sample population differences, as a majority of Li et al.’s patients were ISN/RPS Class III and above. Nonetheless, both Shi et al. and Li et al. found that the degree of tubulointerstitial lesions was negatively correlated with mR2* [25,27]. Given this association and the fact that the degree of tubulointerstitial nephritis in LN is predictive of poor outcomes, mR2* values from BOLD MRI could serve a clinical role in LN patients [28].

Figure 3. Use of blood oxygen level-dependent (BOLD) MRI to visualize lupus nephritis lesions with corresponding biopsy pathology specimens categorized by the International Society of Nephrology and the Renal Pathology Society (ISN/RPS) classes. (a,e,i) Class III; (b,f,j) Class III + V; (c,g,k) Class IV; (d,h,l) Class IV + V. Blue areas in (a–d) indicate low R2* values and oxyhemoglobin levels, with green, yellow, and red areas representing increases in both, in that respective order. Staining in (e–h) was done using Masson’s trichome, and staining in (i–l) was done using Periodic acid-Schiff-methenamine silver. (Figure reprinted with permission from SAGE publishers, from Shi et al., 2018).
5. Discussion

Although BOLD MRI was initially used for cerebrovascular imaging, its use in other organ systems is being increasingly explored. Recent literature demonstrates that BOLD MRI of the kidney has significant potential for clinical and research use (Table 1). Not only is the technology noninvasive, but it also allows clinicians to image and functionally understand renal blood flow and oxygenation without using contrast or radiation. Here, we explored advances made in understanding the technology underlying BOLD MRI for renal studies as well as for its potential diagnostic and clinical role in several nephrotic and nephritic syndromes. For diabetic patients, several studies used BOLD MRI to evaluate diabetic nephropathy progression, but the correlation of R2* values with DN stages yielded mixed results. Two studies that evaluated the effect of diabetic nephropathy treatment on BOLD MRI values differed, finding that lipo-prostaglandin E1 decreased mR2* levels, but that RAAS-modulating drugs did not [21,22]. These inconclusive results demonstrate that more BOLD MRI studies on diabetic nephropathy are needed. In regard to primary nephrotic syndrome, early research is supportive of BOLD MRI’s clinical use, although further research that evaluates each nephrotic syndrome individually (e.g., MGN) is needed, rather than summative analyses. Given the association of nephrotic syndrome with renal hypoxia and BOLD MRI’s utility in assessing intrarenal oxygenation, this technology may serve a role in determining a patient-specific prognosis as well as evaluating progression for those with PNS. Investigations into the utility of using BOLD MRI in nephritic syndrome secondary to lupus nephritis showed promise, as two recent studies found consistent and statistically significant correlations in the ability of BOLD MRI to detect tubulointerstitial pathology in LN patients. This raises the possibility of using the technology to track progression of tubulointerstitial lesions, or even playing a role in establishing the diagnosis. As prognosis and disease physiology in LN can widely differ based on ISN/RPS classification, studies with samples that are more proportionally balanced in terms of disease histopathology are needed to increase validity.

Table 1. Summary of BOLD MRI studies. MG = membranous glomerulonephritis, PNS = primary nephrotic syndrome, DN = diabetic nephropathy, LN = lupus nephritis, NAU = normal to mildly increased albuminuria, MAU = moderately increased albuminuria, TR = repetition time, TE = echo time.

<table>
<thead>
<tr>
<th>Author</th>
<th>Year</th>
<th>Design</th>
<th>Population</th>
<th>TR (ms)/TE (ms)</th>
<th>Disease Stage</th>
<th>eGFR (mL/min/1.73 m²) (Patients, Volunteers)</th>
<th>cR2* (sec⁻¹) (Patients, Volunteers)</th>
<th>mR2* (sec⁻¹) (Patients, Volunteers)</th>
<th>Statistical Analysis</th>
</tr>
</thead>
<tbody>
<tr>
<td>Li et al. [5]</td>
<td>2018</td>
<td>Prospective case-control</td>
<td>9 MG patients, 27 healthy volunteers</td>
<td>100/1.76–18.68</td>
<td>–</td>
<td>–, 110.8 ± 11.2</td>
<td>–</td>
<td>–</td>
<td>Pearson correlation, ANOVA</td>
</tr>
<tr>
<td>Zhang et al.</td>
<td>2015</td>
<td>Prospective case-control</td>
<td>20 PNS patients, 18 healthy volunteers</td>
<td>150/1.6–77.5</td>
<td>–</td>
<td>20.4 ± 3.9, 19.7 ± 0.7</td>
<td>24.0 ± 5.9, 36.5 ± 1.1</td>
<td>Spearman’s correlation coefficient, t-test</td>
<td></td>
</tr>
<tr>
<td>Feng et al.</td>
<td>2020</td>
<td>Retrospective case-control</td>
<td>30 DN patients, 15 healthy volunteers</td>
<td>150/3.4–27.8</td>
<td>NAU, MAU</td>
<td>97.9 ± 8.8, 103.7 ± 11.9 a</td>
<td>17.0 ± 1.9, 16.7 ± 1.6 ab</td>
<td>28.1 ± 3.8, 28.9 ± 3.8 ab</td>
<td>Pearson correlation, ANOVA</td>
</tr>
<tr>
<td>Wang et al.</td>
<td>2011</td>
<td>Prospective non-randomized trial</td>
<td>20 DN patients, 7 healthy volunteers</td>
<td>65/7–53</td>
<td>Mild, moderate-severe</td>
<td>–</td>
<td>13.8 ± 2.4, 19.3 ± 1.2</td>
<td>11.1 ± 0.9, 11.5 ± 0.7</td>
<td>Multiple logistic regression, t-test</td>
</tr>
<tr>
<td>Li et al.</td>
<td>2018</td>
<td>Prospective case-control</td>
<td>16 DN patients,</td>
<td>90/3.29–40.22</td>
<td>Class II–IV</td>
<td>28.4 ± 25.1, –</td>
<td>23.3 ± 6.5, b</td>
<td>29.4 ± 6.7, b</td>
<td>t-test, ANOVA</td>
</tr>
<tr>
<td>Pruim et al.</td>
<td>2013</td>
<td>Prospective randomized two-way crossover study</td>
<td>12 DN patients,</td>
<td>68/6–52.2</td>
<td>–</td>
<td>62.0 ± 22.0, –</td>
<td>17.9 ± 1.5, –</td>
<td>28.7 ± 1.3, –</td>
<td>Spearman’s rank test, ANOVA</td>
</tr>
</tbody>
</table>
Considering that lesions in the glomeruli are primarily in the renal cortex, monitoring changes in cR2* values may appear more appropriate for BOLD imaging of glomerular diseases. However, most studies report a greater statistical significance between mR2* values and disease state compared to cR2* values and disease state. This may be explained by two reasons: The renal medulla receives less blood perfusion compared to the renal cortex, and sodium transporters in the renal medulla exert a high metabolic demand. Pathologic decreases in blood perfusion may result in a lower blood oxygen content, which is exacerbated by high oxygen consumption occurring in the medullary collecting ducts. While the lesions in nephrotic and nephritic syndrome are primarily in the cortex, there may be a pathologic downstream translation to the medulla, which could explain the high medullary signal in the presented data.

Although many of the reported studies are promising, it is important to address several limitations. First, BOLD MRI signals can be affected by factors such as temperature and pH. For example, increased temperature increases oxygen offloading, shifting the oxygenation dissociation curve to the right and causing changes in BOLD signal intensity, independent of perfusion. These distinct influences on oxygen offloading can complicate attempts to associate renal perfusion and BOLD MRI signals [9]. Furthermore, oxygenation, blood flow, sodium transport, and hydration status are all interdependent and any external or internal factors that influence those variables can create noise that interferes with BOLD signals. It is important that these variables are controlled as best as possible prior to proceeding with BOLD MRI, in both research studies and the clinic, for the standardization of results [8,29,30]. Non-oxygenation-related interference factors within BOLD MRI must also be addressed. For example, BOLD signal loss has been documented in neuroimaging, stemming from metal implants such as intracortical electrodes [31]. In renal imaging, the presence of nephrolithiasis or hip arthroplasty can limit visualization of target lesions. Additionally, motion artifacts such as body movement, physiologic noise (such as pulsatile cerebrospinal fluid and arterial blood), and instrumentation noise from scanners can cause interference with BOLD signals [31,32].

MRIs are also expensive and time consuming, limiting the number of participants enrolled in studies [5,11,26,27,29,33,34]. Larger sample sizes are necessary to validate whether BOLD MRI is truly effective in the clinical assessment of renal function in patients with glomerular disease; one study also recommended the use of multicenter randomized controlled trials for external validity of the usage of BOLD MRI [33]. Variability and limitations in imaging techniques within BOLD MRI also limit the internal validity. For example, ROI analysis is commonly used, but is known to have relatively poor levels of inter-observer reliability. Furthermore, in advanced stages of glomerular diseases, the renal cortex and medulla are often difficult to visually distinguish, impairing visualization of the

---

Table 1. Cont.

<table>
<thead>
<tr>
<th>Author</th>
<th>Year</th>
<th>Design</th>
<th>Population</th>
<th>TR (ms)/TE (ms)</th>
<th>Disease Stage</th>
<th>eGFR (mL/min/1.73 m²) (Patients, Volunteers)</th>
<th>cR2* (sec⁻¹) (Patients, Volunteers)</th>
<th>mR2* (sec⁻¹) (Patients, Volunteers)</th>
<th>Statistical Analysis</th>
</tr>
</thead>
<tbody>
<tr>
<td>Li et al. [25]</td>
<td>2014</td>
<td>Retrospective case-control</td>
<td>65 LN patients, 16 healthy volunteers</td>
<td>110/2.2–27.5</td>
<td>Class I–V</td>
<td>11.0 ± 1.6, 12.6 ± 1.4</td>
<td>14.1 ± 3.4, 18.1 ± 2.5</td>
<td>Pearson correlation, t-test</td>
<td></td>
</tr>
<tr>
<td>Rapacchi et al. [26]</td>
<td>2015</td>
<td>Retrospective case-control</td>
<td>10 LN patients, 10 healthy volunteers</td>
<td>187/2.2–43.7</td>
<td>Class III–V</td>
<td>104.7 ± 38.3, 88.3 ± 13.1</td>
<td>–</td>
<td>–</td>
<td>Stepwise logistic regression, unpaired t-test</td>
</tr>
<tr>
<td>Shi et al. [27]</td>
<td>2017</td>
<td>Retrospective case-control</td>
<td>23 LN patients, 10 healthy volunteers</td>
<td>100/2.4–29</td>
<td>Class III–V</td>
<td>102.7 ± 24.8, 112.2 ± 18.8</td>
<td>–</td>
<td>–</td>
<td>Multiple correspondence, ANOVA</td>
</tr>
</tbody>
</table>

* MAU values. NAU values are as follows: estimated glomerular filtration rate (eGFR) 102.02 ± 17.80 (mL/min/1.73m²), cR2* 16.43 ± 2.12 (msec⁻¹), mR2* 34.61 ± 3.39 (msec⁻¹). b (msec⁻¹).
ROI. The use of the TLCO technique has been shown to produce a higher sensitivity and specificity for BOLD imaging in advanced kidney diseases compared to ROI [35].

In conclusion, BOLD MRI has shown promising early results for potential use in clinical practice. While the technology has significant limitations that must be considered, numerous studies have shown encouraging findings that should be further investigated. These advancements in BOLD MRI have the potential to significantly change diagnosis, monitoring, and long-term outcomes of patients with glomerular disease.

Author Contributions: D.R.N., P.G., S.H., R.W. and A.S.T. conceived and outlined the study. D.R.N., P.G., S.H., R.W. and A.S.T. performed a literature search and analyzed the data. D.R.N., P.G., S.H., R.W. and A.S.T. contributed to preparing the manuscript draft. All authors have read and agreed to the published version of the manuscript.

Funding: The authors received no financial support for the research, authorship, or publication of this article.

Institutional Review Board Statement: Not applicable.

Informed Consent Statement: Not applicable.

Data Availability: Sourced data is publicly available in online repositories.

Conflicts of Interest: The authors declare no conflict of interest.

Abbreviations

BOLD MRI  Blood oxygen level-dependent magnetic resonance imaging
CKD  Chronic kidney disease
DN  Diabetic nephropathy
eGFR  Estimated glomerular filtration rate
ISN/RPS  International Society of Nephrology/Renal Pathology Society
LN  Lupus nephritis
mGRE  Multiple gradient-recalled-echo
PNS  Primary nephrotic syndrome
ROI  Region of interest
TLCO  Twelve-layer concentric objects

References


